MEDICAL EQUIPMENT FOR MULTIPLACE HYPERBARIC CHAMBERS Part I: Devices for Monitoring and Cardiac Support

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Kot J: Medical equipment for multiplace hyperbaric chambers. Part I: Devices for monitoring and cardiac support. Europ J Underwater Hyperbaric Med 2005, 6(4): 115-120. All medical devices introduced into the hyperbaric chamber should be of an appropriate design and fit for use in the hyperbaric environment and they should be certified by the manufacturer for hyperbaric conditions. However, until now only several medical devices are CE marked for usage in hyperbaric chambers. Therefore users often need to perform themselves checking of the medical equipment needed for continuation of intensive care during hyperbaric treatment. To make this task easier, this paper presents review of reports of usage of medical devices under increased pressure. Part 1 is concerning devices for monitoring and cardiac support. Part 2 will describe mechanical ventilators and Part 3 will be devoted to infusion pumps and syringes.

Hyperbaric Oxygen Therapy, Medical Equipment, CE Marking

INTRODUCTION

Hyperbaric chamber is an active medical device, which is potentially hazardous taking into accounts its application, and exposure of people inside to increased ambient pressure and increased partial pressure of oxygen. Therefore all hyperbaric systems have to be in accordance with the Council Directive 93/42/EEC of 14 June 1993 concerning medical devices (1). Moreover, according to this Directive all equipment which is introduced into the hyperbaric chamber should be should be certified by manufacturer for hyperbaric conditions and CE marked accordingly covering the hyperbaric environment conditions. Unfortunately, nowadays only several medical devices, which are needed, for continuation of intensive care inside the hyperbaric chamber are marked by manufacturers as compatible with hyperbaric conditions. Therefore users are still forced to perform some checking of devices before putting it into the chamber and usually this is done on the responsibility of the users. Equipment that does not belong to the internal equipment of the chamber and which is not a medical device, should be of an appropriate design and fit for use in the hyperbaric environment up to the maximum working pressure of the chamber it is used within (2).

The general recommendations for medical devices used in hyperbaric chamber systems are presented in the Annex B of the pr14931 "Pressure vessels for human occupancy (PVHO) – Multi-place pressure chamber systems for hyperbaric therapy – Performance, safety requirements and testing" (3), which describes the potential hazards which certain medical devices represent, the risks induced by medical devices likely to be used within hyperbaric chamber systems intended for hyperbaric oxygen therapy and the recommendations for manufacturers of medical devices and users of hyperbaric chamber systems, in order to achieve the highest possible level of safety of the patient and the attendants.

In cases when the medical devices need to be introduced into the hyperbaric environment and it is not certified by the manufacturer for the use in such conditions, the user (personnel of hyperbaric centres) has to check it before installing. The structure of the device is checked from a point of view of raised pressure, of oxygen enriched atmosphere and of electrical supply. Furthermore, the function of the device is checked under hyperbaric conditions to verify the controls, the performances of the device's probes, the operating of the device's built-in electronics, the device's display and the flow rates, pressures and frequencies with which the device dispenses the medical products to the patients.

In case of any doubt, the installation of this medical device in hyperbaric chamber should be abandoned.

To guide medical users, the review of literature is presented here to report medical devices, which have been used under hyperbaric conditions. This is divided into three parts: the part 1 is concerning devices for monitoring and cardiac support, the part 2 will describe mechanical ventilators and the last part 3 will be devoted to infusion pumps and syringes.

MONITORING DEVICES

Monitoring of patophysiological parameters during HBO session strongly depends on severity of the illness and current status of the patient. The set of measured parameters can be as simple as only 3-leads electrocardiography (ECG) up to many critical points of measurement including for example pulmonary capillary wedge pressure (PCWP) or electroencephalography (EEG) (4).

For the safety reasons the optimal method of collecting measurements is to perform acquisition of signals under hyperbaric conditions, transfer it into the electrical signal of low voltage or current and to transfer it out of the chamber through the wall to the outside monitor to be displayed and recorded. The transfer of the signal from the inside to the outside of the chamber can be effectively performed via wire connection or telemetric transmission. The significant disadvantage of the wire connection through the chamber wall is a need for two additional connectors to switch the cable from inside to outside. This may result in decreasing the quality of signal being transmitted, especially with the low signal-to-noise ratio. Transmission using telemetry ensures the continuous monitoring of the patient during all phases of the session including transportation of the patient to and from the chamber. The quality of the signals transmitted depends on the quality of the emitter and receiver, the position of the antenna and the thickness of the chamber wall. Unfortunately, such systems usually allow transmission of only some basic signals, like ECG, with no possibility to transmit more data collected from the patient.

The alternative method is to put the monitoring device under the hyperbaric conditions and to collect, display and record all signals at the patient bed inside the chamber. This solution is easier to be conducted and – in basic version - does not need to make any modification to the existing construction of the chamber. If the user needs, it is possible to collect data inside the hyperbaric chamber and then to send it out of the chamber (again via cable connection through electrical ports or using telemetry) to more sophisticated monitor located outside for further analysis. It is important to remember that introducing of the electrical device inside the chamber increases the risk of fire, and therefore its careful evaluation is obligatory.

The following methods and techniques have been reported to be used safely inside hyperbaric chambers.

Non-invasive monitoring

- A. Electrocardiography. This is the basic monitoring procedure for critically ill patients. The signal can be easily transferred outside the chamber to outside monitor or can be collected by internal one, eg. Propac Encore (5). It includes monitoring of heart rate, analysis of arrhythmias and ST levels, power spectrum analysis of heart rate variability, and tracing of respiration by monitoring the impedance variation between electrodes.
- B. Pulse oximetry. The value of the measurement is restricted to pulse frequency only, as breathing hyperbaric oxygen leads to full saturation of the haemoglobin with only few exception of serious cardiovascular deficiency (6).
- C. Non-invasive blood pressure. This can be done manually using method of auscultation of blood noises. On the other hand, automatic method based on oscillation analysis needs to place the electrical pump for inflation of the arm cuff inside the chamber to ensure working at the same pressure. It posses an additional hazard for fire and therefore careful examination of the mechanism is necessary prior to the usage inside the hyperbaric chamber, including a replacement of pump motor with brushless type in some cases, e.g. Propac Encore (5). Until now there is no reference in the literature about the influence of increased density of air used for inflation of the cuff on the accuracy of the blood pressure measurement or on the workload for the pumping systems.
- D. Temperature. It can be easily measured at any point by the electrical termistors and signals can be sent to any device used for critical monitoring. The mercury thermometries must not be entered into the hyperbaric chambers due to the toxicity of mercury under hyperbaric conditions.

- E. Transcutaneous partial pressure of the oxygen (TcPO₂). It is used for evaluation of oxygenation of the local tissues as result of vascular system and efficacy of the hyperbaric therapy (7). Moreover, it can be used for quality assurance system giving independent measurement of the dose of oxygen absorbed by the patient leading to early detection of any leakage in breathing systems. Together with measurement of the transcutaneous partial pressure of the carbon dioxide (TcPCO₂) it is used for control of ventilation / perfusion status of the patient (8, 9). The sensors are connected to the patient skin and electrical signal from sensors is redirected to the internal or external display.
- F. Electroencephalography (EEG). It can be acquired safely using computerized multi-channel systems to avoid any artefacts (10, 11). Usually the signal obtained from head sensors is transferred out of the chamber to the external computer for further evaluation (eg. spectral analysis).
- G. Evoked potentials (EP). The usage of potentials evoked at a cortical and brainstem level by acoustic, visual and somatosensorial stimuli in humans during hyperbaric session have been described (10, 12) and it has been used for research purposes up to 62.5 ATA (13).
- H. Laser-Doppler flowmetry (LDF). It is used for assessment of peripheral microcirculation and is suitable for non-invasive monitoring of skin perfusion under hyperbaric conditions (14, 15).
- I. Trans-thoracic bioimpedance. It can be used for noninvasive estimation of cardiac output (CO) and extravascular lung water (ELW). Regardless of doubts arising for accuracy of this method in measurement of cardiac output in haemodynamically unstable patients, it has been validated in hyperbaric environment using the NNCCM3 Bohmed (16, 17, 18).
- J. Echocardiography and Doppler studies. It can serve for non-invasive monitoring of haemodynamic status of the patient (19). It can be performed under hyperbaric conditions with any equipment providing that signals from probes are directed outside the chamber through signal ports (20).
- K. Transcranical Doppler. The Doppler probe can be placed at the patient in the hyperbaric chamber and signal is transferred by wires to the outside of the chamber. This technique was used up to 4 ATA (8, 21).
- L. Near infrared spectroscopy (NIRS). It can be used for measurement of regional oxygenation of tissues. A transcranial regional cerebral oxygenation using INVOS 3100 cerebral oximeter (placed outside the chamber) has been reported to be measured under hyperbaric conditions up to 2.5 ATA with only sensor inside the chamber (22), as well as during pressurization in portable chamber at high altitude (23).
- M. Spirometry and airway pressure. Measurement of the airway pressure and the exhaled tidal volume (minute volume) is an absolute minimum set of monitoring of patients ventilation during artificial ventilation under hyperbaric conditions. The mechanical spirometers

are extensively used in hyperbaric chambers due to their simplicity. The electric spirometer Ohmeda 5420 has been used successfully up to 6 ATA (24).

N. Breathing gas analysis. According to some authors to ensure that patient receives the correct dose of oxygen, breathing gas analysis should be performed continuously during every HBO session (25), with measurement of transcutaneous partial pressure of oxygen being an alternative (26, 27). The oxygen content in the breathing mixture can be measured at any point of the breathing system, including inspiratory line (27), space under mask or hood (25) or expiratory line (25, 28). The expired gas can be analysed for end tidal carbon dioxide partial pressure as a part of monitoring of the patient's ventilation (21). The mainstream determination is subjected to errors due to "pressure broadening effect" produced by the increased density of gas. As a result falsely high values of the patient's ETCO2 are usually reported, which need to be corrected using mathematical equations (29, 30). Alternatively a sidestream analysis can be performed easily and reliably outside the chamber using decompressed expiratory gas. The usage of mass spectrometry for analysis of decompressed gas samples has been reported (31, 32, 33), however due to costly equipment it was mainly used for research purposes.

Invasive monitoring

- A. Blood pressure (BP). Blood pressure can be measured invasively in any blood vessel providing that transducer is placed under the hyperbaric conditions, correctly filled and calibrated (34). Using that method one can measure pressure in the central venous system (CVP), arterial system (ABP) and pulmonary arteries (PAP, PCWP). Regardless the clinical safety of the patient, the careful elimination of all gas bubble, which may collect at the diaphragm, is a must to ensure the stability of the pressure readout.
- B. Cardiac output (CO). Methodology and calculations for the cardiac output measurement by Swan-Ganz catheter using thermodilution is unchanged under hyperbaric conditions (16, 35, 36). The Edwards American Laboratories module for measurement of CO has been used in hyperbaric chamber (16).
- C. Intracranial pressure (ICP). It can be conducted using fluid-filled systems or tip transducer systems. Fluidfilled system is based on a catheter placed in the region of the brain being monitored and transducer located outside the skull similarly to the blood pressure measurement system (34, 37). In the tip transducer system the miniaturised pressure transducer is located just at the site of measurement and only the read-out signal is transferred outside the scull to the monitoring device (eg. via the fibre optic) (34). Whole system for fibre optic measurement of the ICP from Camino Laboratories (San Diego, CA, USA) has been used in hyperbaric chamber (34). Both systems for measurement of ICP can be used safely under hyperbaric conditions providing the general electrical safety for the monitoring device.

- D. Blood gas analysis (ABG). In order to receive the exact results of blood gas analysis it is necessary to measure it inside the hyperbaric chamber, as there are problems with accurate calibration of the blood gas analysers for gas tensions higher than ambient pressure (38). On the other hand, using some calculations, it is possible to get reliable results of normobaric blood measurement gas after decompression of the sample (39). The IL-813 and IL-1306 models (Instrumentation Laboratory Inc., USA) were used in the hyperbaric chamber with no technical problem under pressure of 2 and 3 ATA, respectively (40, 41). Also a portable blood gas analyser (StatPal II, PPG Industries, La Jolla, CA, USA) has been developed to operate under pressure and it has been successfully tested up to 2 ATA (42, 43).
- E. Venous saturation of the blood (SvO₂). It is method used to detect early onset of general or local ischaemia. The catheter equipped with the fiber optic to measure the saturation of the blood *in situ* can be placed in pulmonary artery or vena cava to measure global ischaemia or in jugular or hepatic vein to measure specific organ ischemia. Regardless of the electrical safety of the monitoring device inside the hyperbaric chamber, the main problem which exists with this method is calibration of the system under pressure (44).
- F. Tissue oxygenation. A multi-parameter sensor NeuroTrend (Codman, Johnson&Johnson Professional, Inc., MA, USA) can be used for a direct measurement of tissue oxygenation (45). The probe and a satellite monitor have been adapted for the hyperbaric conditions. It is designed for measurement of brain tissue oxygenation and it has been tested experimentally up to 3 ATA.
- G. Blood glucose level. The blood glucose level can be significantly decreased during the HBO session (46) and therefore its measurement is of critical value. Several models of glucometers using different methods of measurements have been tested under hyperbaric conditions: Chemstrips (47), Glucometer M+, Companion 2, HemoCue, OneTouch II, ExacTect Pen (48), Bayer Glucometer 4 (49). The general conclusion is that measurement of the glucose level is affected in the hyperbaric chamber giving falsely high readouts especially at low glucose levels.

CARDIAC SUPPORT

Defibrillation

Sudden cardiac death commonly results from ventricular tachycardia or fibrillation, and early defibrillation is the single most important determinant of survival for those patients (50). For every minute of sustained cardiac arrest, survival decreases by 10%. Therefore, the possibility to use defibrillation in hyperbaric environment is a logical consequence of treating critically ill patients in hyperbaric chambers. The procedure of defibrillation is inherently dangerous to use in hyperbaric chambers because of the danger of fire caused by electrical discharges and voltaic arc, which may be generated between the paddles. Therefore this procedure is absolutely contraindicated in

the pure oxygen atmosphere of the monoplace chamber (51). On the other hand, in multiplace chamber defibrillation can be performed relatively safely, if several precautions are taken:

- 1. The chamber is compressed with air and oxygen is kept below 21.5% (52).
- 2. Large surface adhesive plates are attached to the patient's chest (53, 54). The gel is applied to assure conductive bridge between the skin and the plates, and the area around the plates is kept free from flammable materials (55).
- 3. Transmission cable of wide diameter and low resistance passes through the chamber wall outside (54).
- 4. The defibrillator (including switches) is located outside (52, 53, 54, 55).
- 5. Three persons are needed to perform the operation: 1) medical attendant inside the chamber is responsible for attaching paddles; 2) an external defibrillator's operator is controlling the discharge unit located outside the chamber and 3) chamber operator is ready for immediate activation of water-deluge fire suppression system (52).

The data concerning the use of defibrillation in patients inside the hyperbaric chambers is scarce. The experiments of defibrillation were conducted with swine model of resuscitation in controlled environment up to 6 ATA without any incidents in 270 defibrillations (52, 56). Interestingly, luminous spark were seen in dark environment under the electrode plates during defibrillation with 200 to 360 joules at ambient pressure, while no spark was apparent under hyperbaric conditions, probably due to compression of endogenous gas in the electrode gel (57). When following presented rules the risk of fire is kept on the acceptable low level, so general opinion is that the defibrillation may be performed safely in the multiplace chamber (51, 52). If technically impossible to be conducted under hyperbaric conditions, defibrillation is performed after emergency surfacing of patient from hyperbaric chamber to outside assuming that preoxygenation with hyperbaric oxygen gives few minutes more before brain death occurs.

External Pacing

Some temporary external pacemakers have been reported to malfunction under hyperbaric conditions (58, 59), some others have been shown to function satisfactorily up to 8.7 ATA (60). Therefore the use of untested external pacemakers should be avoided, and other alternatives should be used in case of need. One is to locate the pacemaker outside the chamber (55) and to transfer wires through the wall similarly to defibrillation described above. The other is to use permanent hermetically sealed pacemaker attached to the patient's temporary external leads (58) or to the catheter based wires.

Implanted Pacemakers

The number of patients with implanted pacemakers (PM) and automatic implanted cardiac defibrillators (AICD) treated inside hyperbaric chambers for other medical reasons is growing.

According to general opinion, internal cardiac pacemakers are unaffected by the hyperbaric environment (61), however – obviously – it can be true only for limited range of pressures. Most implanted devices are rated to at least 2.4 ATA (62, 63), but some authors reports that all pacemakers tested by them were adequate to treatment pressure below 3 ATA, and some even to 7 ATA (64). During the ISO-compatible ETO-standard sterilization process the pressure is up to 2.5 ATA, therefore all devices sterilized by this method are unintentionally tested for such overpressure (65).

Nevertheless, it is highly advisable to constantly monitor ECG of patients with implanted pacemakers and cardiac defibrillators during every HBO session.

The list of PMs and AICDs tested in hyperbaric chamber is presented in the Table 1.

Manufacturer	Device	Checking conditions
Biotronik GmbH	PM: All models developed until 1999	2.5 ATA, but not for 6.0 ATA (62,

Table 1. Pacemakers and automatic implanted cardiac defibrillators used in multiplace hyperbaric chambers.

PM: All models developed until 1999	2.5 ATA, but not for 6.0 ATA (62,
-	65, 66)
PM: INOS CLS, INOS plus CLS	6.0 ATA (65, 66)
IS-1-Connector	6.0 ATA (67)
AICD: Phylax AV	6.0 ATA (66)
Pulse generator and AICD	2.36 ATA; anecdotally more (55)
PM: model 0503	7.9 ATA (58)
PM: Quantum (254-20), Nova II (281-05), Cornos	5.78 ATA for 24 h (55)
(282-04), Relay (294-03)	
PM: models 253-02, 259-01	7.9 ATA (58)
PM: Legend TM, Legend II TM, Synergist II TM,	2.8 ATA (55)
Elite TM, Thera I, Prodigy, Eilte II	
PM models: 5950, 5951, 5985, 5973, 5989	7.9 ATA (58)
External PM: #5388	8.7 ATA (68)
	2.5 ATA (as declaration of
	manufacturer) (65)
PM: All models developed until 1999	6.8 ATA (55, 65)
PM: Syncrony III	6.8 ATA (65)
PM: model Vivelith 5	7.9 ATA (58)
	PM: INOS CLS, INOS plus CLSIS-1-ConnectorAICD: Phylax AVPulse generator and AICDPM: model 0503PM: Quantum (254-20), Nova II (281-05), Cornos (282-04), Relay (294-03)PM: models 253-02, 259-01PM: Legend TM, Legend II TM, Synergist II TM, Elite TM, Thera I, Prodigy, Eilte IIPM models: 5950, 5951, 5985, 5973, 5989External PM: #5388PM: All models developed until 1999PM: Syncrony III

REFERENCES

- Council Directive 93/42 of June 1993 concerning medical devices. NoL 169/1 - 169/43, 12 July 1993.
- COST B14. Working Group «Safety» European Code of Good Practice for Hyperbaric Oxygen Therapy (May 2004). EJUHM 2004; 5(suppl. 1): 1-68. Available at: http://www.oxynet.org.
- prEN14931:2004 "Pressure vessels for human occupancy (PVHO) – Multi-place pressure chamber systems for hyperbaric therapy – Performance, safety requirements and testing". European Committee for Standardisation (CEN), Brussels, Belgium.
- Rogatsky GG, Shifrin EG, Mayevsky A. Physiologic and biochemical monitoring during hyperbaric oxygenation: a review. Undersea Hyperb Med. 1999 Summer; 26(2): 111-122.
- 5. US NEDU. Hyperbaric-Safe Medical Equipment 2005. http://www.supsalv.org/nedu/ hyperbaric-safe-list.htm.
- Oriani G, Rosetti M, Meazza D, Sacchi C, Ronzio A, Campagnoli P. A rational approach to monitoring in a hyperbaric environment. Acta Anaest Ital 1991; 42(suppl.2): 157-158.
- Wattel FE, Mathieu DM, Neviere RR. Transcutaneous oxygen pressure measurements. A usefull technique to appreciate the oxygen delivery to tissues. J Hyperbar Med 1991; 6: 269-282.
- Omae T, Ibayashi S, Kusuda K, Nakamura H, Yagi H, Fujishima M. Effects of high atmospheric pressure and oxygen on middle cerebral blood flow velocity in humans measured by transcranial Doppler. Stroke. 1998 Jan; 29(1): 94-97.
- 9. Tabrah FL, Tanner R, Vega R, Batkin S. Baromedicine today – rational uses of hyperbaric oxygen therapy. Hawaii Med J 1994; 53: 112-115, 119.
- Kawamura S, Ohta H, Suzuki A, Nemoto M, Hinuma Y, Suzuki E, Yasui N. [Reproducibility of somatosensory evoked potentials and EEG in normal humans under hyperbaric oxygenation] No To Shinkei. 1987 Mar; 39(3): 243-250.
- Longoni C, Marchesi G. Adapting the hyperbaric chamber to the health care environment: history and future trends. In Handbook on hyperbaric Medicine. G. Oriani, A. Marroni, F. Wattel (Eds.). Springer-Verlag, Berlin, 1995: 741-764.
- Litscher G, Friehs G, Maresch H, Pfurtscheller G. Electroencephalographic and evoked potential monitoring in the hyperbaric environment. J Clin Monit. 1990 Jan;6(1):10-17.
- Lorenz J, Athanassenas G, Hampe P, Plath G, Wenzel J. Human brainstem auditory-evoked potentials in deep experimental diving to pressures up to 62.5 bar. Undersea Biomed Res. 1992 Sep; 19(5): 317-330.
- Ratzenhofer-Komenda B, Kovac H, Smolle-Juttner FM, Friehs GB, Schwarz G. Quantification of the dermal vascular response to hyperbaric oxygen with laser-Doppler flowmetry. Undersea Hyperb Med. 1998 Winter; 25(4): 223-227.
- Litscher G, Moeller KO, Ratzenhofer-Komenda B, Schwarz G, Koop T, Kovac H. Laser Doppler flowmetry in the hyperbaric environment. Lasers Med Sci 1997; 12: 342-346.
- Pelaia P, Rocco M, Conti G, De Blasi RA, Bufi M, Antonelli M, Bortone C. Hemodynamic modifications during hyperbaric oxygen terapy. J Hyperbar Med 1992; 7(4): 229-237.
- Pelaia P, Rocco M, Malpieri R, Bortone C. Validation of a non invasive haemodynamic monitoring by the transthoracic impedance with the termodilution method in the hyperbaric chamber. EUBS Basel, Switzerland 1992: 49-50.

- Villanucci S, Di Marzio GE, Scholl M, Pivorine C, d'Adamo C, Settimi F. Cardiovascular changes induced by hyperbaric oxygen therapy. Undersea Hyperbar Med. 1990; 17(suppl): 117.
- Nürnmerg JH, Staschen CM, Bettinghausen E. Noninvasive hemodynamic monitoring in hyperbaric chambers: application of a non-imaging Doppler device. EUBS Basel, Switzerland 1992: 140.
- Molenat F, Boussuges A, Grandfond A, Rostain JC, Sainty JM, Robinet C, Galland F, Meliet JL. Haemodynamic effects of hyperbaric hyperoxia in healthy volunteers: an echocardiographic and Doppler study. Clin Sci (Lond). 2004 Apr; 106(4): 389-395.
- Visser GH, Van Hulst RA, Wieneke GH, Van Huffelen AC. Transcranial Doppler sonographic measurements of middle cerebral artery flow velocity during hyperbaric oxygen exposures. Undersea Hyperb Med. 1996 Sep; 23(3): 157-165.
- Litscher G, Schwarz G, Ratzenhofer-Komenda B, Kovac H, Gabor S, Smolle-Juttner FM. Transcranial cerebral oximetry in the hyperbaric environment. Biomed Tech (Berl) 1997; 42(3): 38-41.
- Imray CH, Clarke T, Forster PJ, Harvey TC, Hoar H, Walsh S, Wright AD; Birmingham Medical Research Expeditionary Society. Carbon dioxide contributes to the beneficial effect of pressurization in a portable hyperbaric chamber at high altitude. Clin Sci (Lond). 2001 Feb; 100(2): 151-157.
- Youn BA, Myers RA. Volume monitor for mechanical ventilation in the hyperbaric chamber. Crit Care Med. 1989 May; 17(5): 453-454.
- Stephenson RN, Mackenzie I, Watt SJ, Ross JA. Measurement of oxygen concentration in delivery systems used for hyperbaric oxygen therapy. Undersea Hyperb Med. 1996 Sep; 23(3): 185-188.
- COST B14 WG B. Research Quality Guidelines. Working Group B Final Report, December 2000. http://www.oxynet.org/02COSTinfo/guidlines.htm.
- VDD after Almeling M. Welslau W, Hampe P, Hock L, Niklas A. Online measurement of oxygen consumption during HBO therapy. EUBS Stockholm, Sweden 1998: 187.
- Neirynck Y, Houman R, Germonpre P. Expired oxygen measurement during hyperbaric oxygen therapy. EUBS Brugges, Belgium 2002: 129-132.
- Swaby G, Brown S, Sutton T, Love T, Fife CE. Calibration of an end tidal CO2 monitor under hyperbaric conditions. Undersea Hyperbar Med 1996; 23(suppl): 79.
- Handell S, Ansjon R, Casto R, Lind F. Respiratory CO2 monitoring of the critically ill patient in the multiplace chamber. EUBS Basel, Switzerland 1992: 59-61.
- Mathieu D, Neviere R, Wattel F. Measurement of metabolic gas exchange and minute ventilation in hyperbaric atmosphere using a mass spectrometer alone. EUBS Crete, Greece 1991: 271-269.
- 32. Richard RB, Loomis JL, Russell GB, Snider MT. Breathby-breath monitoring of respiratory gas concentrations during compression and decompression. Undersea Biomed Res. 1991 Mar; 18(2): 117-126.
- 33. Arieli R, Daskalovic Y, Eynan M, Arieli Y, Ertracht O, Shupak A. Use of QP 900 mas spectrometer for direct gas sampling from the high pressure chamber. EUBS Haifa and Eilat, Israel 1999: 266-269.
- Pelaia P, Rocco M, Di Lauro E, Spadetta G. Safety and HBO Therapy. In Handbook on hyperbaric Medicine. G. Oriani, A. Marroni, F. Wattel (Eds.). Springer-Verlag, Berlin, 1995: 715-736.
- 35. Mathieu D, Neviere R, Wattel F. Haemodynamic monitoring during HBO, technical and safety aspects Acta

and intensive care in Italy. Acta Anaest Ital 1991; 2(suppl): 42.

- Wattel F, Mathieu D, Neviere R. Invasive vs non-invasive haemodynamic monitoring. Acta Anaesthesiol Ital. 1991; 42(suppl 2): 164-166.
- Kohshi K, Yokota A, Konda N, Kinoshita Y, Kajiwara H. Intracranial pressure responses during hyperbaric oxygen therapy. Neurol Med Chir (Tokyo). 1991 Sep; 31(9): 575-581.
- Camporesi EM, Richard EM. Management of critically ill patients in the hyperbaric environment. MEDSUBHYP 1987; 6(3): 80-83.
- Weaver LK, Howe S. Normobaric measurement of arterial oxygen tension in subjects exposed to hyperbaric oxygen. Chest. 1992 Oct; 102(4): 1175-1181.
- Suzuki E, Ohta H, Hinuma Y, Hadeishi H, Kawamura S, Nemoto M, Yasui N. Arterial blood-gas analysis under hyperbaric conditions. 10th International Congress on Hyperbaric Medicine, Amsterdam, The Netherlands 1991: 175-178.
- 41. Doar PO, Boso A, Alford E. Evaluation of modern blood gas analysers for hyperbaric conditions. Undersea Hyperbar Med 1996; 23(suppl): 66.
- 42. Sutton T, Freeses M, Saur S, Swaby G, Fife CE, Berry J. Testing of a portable blood gas analyser under hyper/hypobaric conditions. UHM 1994; 21(suppl): 50.
- 43. Wong RJ, Mahoney JJ, Harvey JA, Van Kessel AL. Stat Pal II pH and blood gas analysis system evaluated. Clin Chem. 1994; 40: 124-129.
- 44. Gismondi A, Caione R, Scardia M, De Razza L. SvO2 monitoring in hyperbarism: a preliminary study. Acta Anaest Ital. 1991; 42(suppl 2): 157-158.
- Henze D, Bomplitz M, Radke J, Clausen T. Reliability of the NeuroTrend sensor system under hyperbaric conditions. J Neurosci Methods. 2004 Jan 15; 132(1): 45-56.
- 46. Springer R. The importance of glucometer testing of diabetic patients pre and post dive. Undersea Hyperbar Med 1990; 18(suppl): 20.
- 47. Zel G. Inaccuracies of blood sugar determinations in the hyperbaric environment using Chemstrips. Undersea Hyperbar Med 1987; 14(2 suppl): 20.
- Price ME Jr, Hammett-Stabler C, Kemper GB, Davis MG, Piepmeier EH Jr. Evaluation of glucose monitoring devices in the hyperbaric chamber. Mil Med. 1995 Mar; 160(3): 143-146.
- 49. Edge CJ, Grieve AP, Gibbins N, O'Sullivan F, Bryson P. Effects of pressure on whole blood glucose measurements using the Bayer Glucometer 4 blood glucose meter. Undersea Hyperb Med. 1996 Dec; 23(4): 221-224.
- Varon J, Sternbach GL, Marik PE, Fromm RE Jr. Automatic external defibrillators: lessons from the past, present and future. Resuscitation. 1999; 41(3): 219-223.
- Weaver LK: Management of critically ill patients in the monoplace hyperbaric chamber, Hyperbaric Medicine Practice. EP Kindwall EP (Ed). Flagstaff, Best Publishing, 1995, pp 174-246.
- 52. Swanson HT, Sheps S, VanMeter KW. Use of defibrillators in the hyperbaric chamber. UHM 1999; 26(suppl): 54.
- Longoni G, Marchesi G. Adapting the hyperbaric chamber to the health care environment: History and future trends. In Handbook on Hyperbaric Medicine. G. Oriani, A. Marroni, F. Wattel (Eds.). Springer-Verlag, Berlin, 1996: 741-764..
- Martindale LG, Milligan M, Fries P. Test of an R-2 Defibrillator adapter in the hyperbaric chamber. J Hyperbar Med, 1987; 2: 14-25.
- 55. Ratzerhofer-Komenda B, Kemmer A. HBO in intensive care. Proceedings of the 7th European Consensus

Conference on Hyperbaric Medicine. Lille, France 2004: 107-121.

- 56. Van Meter KW, Swanson HT, Sheps S, Ross D, Harch PG, Simanonok J, Buechter K, McSwain N, Kriedt F, Gottlieb SF, Gonzalez R, Anstadt G. A pilot study to determine the safety and practicality of using a single human resuscitator for ADMVAD assisted ACLS after a 15 minute ventricular fibrillation in swine in a hyperbaric chamber at 1.0, 2.8, and 6.0 ATA/abs. Undersea Hyperbar Med 1996; 23(suppl): 69.
- 57. VanMeter KW, Kreidt F, Swanson HT, Wilson JP, Nolan TA, Moises JP, Harch PG, Van Every M, Barratt DM. Development of an experimental model for ventilation of swine undergoing closed chest advanced cardiac life support (ACLS) with 100% oxygen in normobaric and hyperbaric environment after a prolonged cardiopulmonary arrest using external cardiac electrodes for both pacing and defibrillation (EPD) while monitoring brain oxygenation by non-invasive brain niroscopy. UHM 2000; 27(suppl): 54.
- Kratz JM, Blackburn JG, Leman RB, Crawford FA. Cardiac pacing under hyperbaric conditions. Ann Thorac Surg. 1983; 36(1): 66-68.
- 59. Tomatis L, Nemiroff M, Riahi M, Visser J, Visser E, Davies A, Helentjaris D, Stockinger F, Kanten D, Oosterheert M, Valk A, Blietz D. Massive arterial air embolism due to rupture of pulsatile assist device: successful treatment in the hyperbaric chamber. Ann Thorac Surg. 1981; 32(6): 604-608.
- Pressley CC, Chen H, Doar PO, Moon RE. External cardiac pacemaker under hyperbaric conditions. UHM 1999; 26(suppl): 54.
- Kindwall EP. Contraindications and side effects to hyperbaric oxygen treatment. In EP Kindwall (ed) Hyperbaric Medicine Practice. Best Publishing Company, Flagstaff, USA 1999; 83-98.
- 62. Simmons S, Zmaeff J. Review of implanted cardiac rhythm devices in the hyperbaric chamber. UHM 2001; 28(suppl): 101
- Simmons S, Zmaeff J. Review of implanted cardiac rhythm devices in the hyperbaric chamber. UHM 2001; 28(suppl): 84-85.
- 64. Simmons S. Review of permanent pacemakers in hyperbaric chambers. UHM 1998; 25(suppl): 14.
- 65. Wonhas C, Wonhas-Thiele H. Safety in hyperbaric oxygen therapy (HBO) also for patients with implanted pacemakers (PM)?. UHM 1998; 25(suppl): 15.
- Wonhas C, Wonhas-Thiele H, Mueller A. Implanted cardiac defibrillator (ICD) and pacemaker (PM) after longtime hyperbaric oxygen therapy (HBO) – Biotronik Phylax AV (ICD) and INOS PLUS CLS (PM). UHM 2000; 27(suppl): 32.
- Wonhas C, Wonhas-Thiele H. Cardiac pacemakers (PM) and hyperbaric Oxygen Therapy (HBO) – IS-1-Connector and Biotronik INOS CLS pacemaker. UHM 1999; 26(suppl): 54.
- Pressley CC, Chen H, Doar PO, Moon RE. External cardiac pacemaker under hyperbaric conditions. UHM 1999; 26(suppl): 54.

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